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(73) Proprietor: Takeda Chemical Industries, Ltd.
1-1, Doshomachi 4-chome
Chuo-ku, OSAKA (JP)

(72) Inventor: Yamada, Minoru
1-8, Yuyamadal 1-chome
Kawanishi,
Hyogo 666-01 (JP)
Inventor: Ishiguro, Seiko
2-86, Seiwadainishi 3-chome
Kawanishi,
Hyogo 666-01 (JP)
Inventor: Ogawa, Yasuaki
77-42, Koaza-tanita,
Aza-ohyamazaki
Ohyamazaki-cho,
Otokuni-gun,
Kyoto 618 (JP)

(74) Representative: Lewin, John Harvey
Elkington and Fife
Prospect House
8 Pembroke Road
Sevenoaks, Kent TN13 1XR (GB)

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EP 0 481 732 B1

Description

FIELD OF THE INVENTION

5 The present invention relates to a prolonged release preparation and polymers for said preparation.

BACKGROUND OF THE INVENTION

Biodegradable polymers can be used as bases for pharmaceutical preparations such as microcapsules.
 10 Such a biodegradable polymer is disclosed in Japanese Kokai Patent Application No. 61-28521 (the corresponding U.S. Patent Nos. 4677191 and 4683288) which teaches that the polycondensation reaction of lactic acid and/or glycolic acid, in the presence or absence of a catalyst, gives rise to such a polymer or copolymer.

Japanese Patent Publication No. 1-57087 (the corresponding U.S. Patent Nos. 4652441, 4711782 and
 15 4917893) discloses a method of manufacturing sustained-releasing microcapsules employing such biodegradable polymers.

Japanese Kokai Patent Publication No. 62-54760 (the corresponding U.S. Patent Nos. 4728721 and 4849228) mentions that the initial drug release pattern of microcapsules can be improved by washing a biodegradable polymer solution with water to remove the water-soluble low molecular fraction.

20 Japanese Kokai Patent Publication No. 2-212436 describes a prolonged release pharmaceutical polymer available on direct dehydrative polycondensation of lactic acid and/or glycolic acid with a hydroxycarboxylic acid.

EP-A-0 263 490 and JP 02,212436 disclose the use of copolymers of glycolic acid and an α -hydroxycarboxylic acid as biodegradable carrier for drugs.

25 EP-A-0 281 482 discloses poly blends for selective biodegradability. Predetermined or preselected biodegradation rates can be achieved by selection of appropriate blend components. One example is a blend of poly(ϵ -caprolactone) and poly(L-lactic acid-co-glycolic acid).

In a prolonged release preparation comprising a dispersion of a drug substance in a biodegradable macromolecular compound, it is preferable that the rate of drug release can be controlled as desired.
 30 Generally the period of release of such a prolonged release preparation is controlled by adjusting the monomer composition and molecular weight of the biodegradable polymer used for the preparation. The rate of drug release is preferably constant over the entire period of release. As mentioned hereinbefore, many proposals have been made for improving the initial release pattern of this type of preparation. However, when the designed release period is comparatively short, it is frequently encountered that the
 35 drug is released en masse in the second half of the release period. Furthermore, the composition and molecular weight of the biodegradable polymer must be optimized for each drug used and each designed release period and this optimization requires much time and effort.

Furthermore, it is difficult to obtain a constant drug release pattern by using a preparation mixing two kinds of microcapsule which have different release periods, since the drug release pattern of the mixed
 40 preparation is apt to change discontinuously in the course of the drug release.

The inventors of the present invention explored into this field of technology for overcoming the above-mentioned disadvantages and found that when the period of drug release is controlled using a simple blend of a biodegradable polymer having a comparatively low degradation rate and a biodegradable polymer having a comparatively high degradation rate, the release characteristic of the system in the second half of
 45 the release period is remarkably improved over that of a system employing a copolymer of the same monomer composition. The present invention is predicated on the above finding.

SUMMARY OF THE INVENTION

50 The present invention is accordingly directed to (1) a polymer for a prolonged release preparation comprising a polylactic acid (A) and a copolymer (B) between glycolic acid and a hydroxycarboxylic acid of the formula (I)

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wherein R means an alkyl group containing 2 to 8 carbon atoms as blended in a weight ratio of 10/90 through 90/10 and (2) a prolonged release preparation containing an effective amount of a water-soluble drug substance in said polymer (1).

5 DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

The molecular weight in this specification means the polystyrene equivalent molecular weight as determined by gel permeation chromatography (GPC) using polystyrene as the reference standard. In the determination of molecular weights, the GPC column KF804L x 2 (Showa Denko) and, as the mobile phase, chloroform were used.

The polylactic acid used in the present invention may be any of the L-, D- and D,L-polylactic acid but when a solvent is used in the formulation, the mole ratio of D- and L-lactic acid in the D,L-polylactic acid is usually 75/25 to 25/75, preferably 48/52 to 25/75, more preferably 45/55 to 25/75 from the standpoint of solubility. It is also preferable to use a polylactic acid which has a molecular weight peak value of 5000 to 30000 and shows, when used alone, a release period of about 2 to 4 months.

Two methods are known for the synthesis of said polylactic acid, namely the ring-opening polymerization of lactide which is a dimer of lactic acid and the dehydrative polycondensation of lactic acid. For the preparation of a comparatively low molecular weight polymer for use in the present invention, the direct dehydrative polycondensation of lactic acid (cf. Japanese Kokai Patent Application No. 61-28521) is easier to carry out.

Referring to the copolymer (B), the constituent hydroxycarboxylic acid of general formula (I) includes, among others, 2-hydroxybutyric acid, 2-hydroxyvaleric acid, 2-hydroxy-3-methylbutyric acid, 2-hydroxycaproic acid, 2-hydroxyisocaproic acid, 2-hydroxycaprylic acid and so on. Particularly preferred is 2-hydroxybutyric acid. These 2-hydroxycarboxylic acids may each be D-, L- or D,L-configured but the D,L-compound is preferably used. The mode of copolymerization of the copolymer (B) may be random, block or graft. Among such glycolic acid copolymers, those which are degraded in the body with comparative rapidity and releases, when a preparation was made alone, a water soluble drug within not longer than one month are preferred.

The preferred proportion of glycolic acid (I) in the copolymer (B) is in the range of 40 to 70 mole % of glycolic acid and the proportion of the hydroxycarboxylic acid is in the range of 60 to 30 mole %, respectively. If the proportion of glycolic acid is less than 40 mole %, the pattern of drug release may not be linear, while the use of more than 70 mole % of glycolic acid makes the copolymer hardly soluble in a solvent, thus making it difficult to manufacture the preparations. Moreover, the glycolic acid copolymer preferably has a molecular weight peak value of 5000 to 20000 as determined by GPC.

A method for synthesis of said glycolic acid copolymer (B) has been described for glycolic acid-L-leucinic acid copolymer in Japanese Kokai Patent Publication No. 2-212436. However, the copolymer (B) can be easily synthesized by the general synthetic methods. (e.g. Japanese Kokai Patent Application No. 61-28521).

In the pharmaceutical base according to the present invention, polylactic acid (A) and glycolic acid copolymer (B) can be used in a blend ratio of 10/90 through 90/10 (by weight), preferably 25/75 through 75/25 (by weight). If the proportion of either component is excessive, the resulting therapeutic system will have a release pattern not much different from the system exclusively composed of the one component and fail to show the desired linear second-half release characteristic. The method of blending is optional.

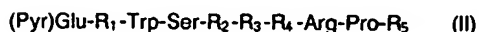
The biodegradable polymer composition thus obtained can be used as the pharmaceutical base for prolonged release preparations such as microcapsules.

The water-soluble drug substance which can be incorporated in the above preparations includes those substances which are highly hydrophilic and have low oil-water partition coefficients. The low oil-water partition coefficient means that the coefficient of partition between octanol and water, for instance, is not higher than about 0.1.

While the kinds of such water-soluble drug substances are virtually not limited, there may be employed a variety of physiologically active peptides, antibiotics, antitumor agents, antipyretics, analgesics, antiinflammatory agents, antitussive-expectorants, sedatives, muscle relaxants, antiepileptics, antiulcer agents, antidepressants, antiallergic agents, cardiotonics, antiarrhythmic agents, vasodilators, hypotensive diuretics, antidiabetic agents, anticoagulants, hemostatic agents, antituberculous agents, hormones, narcotic antagonists bone resorption inhibitors, angiogenesis-inhibiting substances and so on.

The physiologically active peptide which is used in the present invention is one consisting of two or more amino acid residues and preferably has a molecular weight of about 200 to 80000.

As examples of such peptides there may be mentioned luteinizing hormone-releasing hormone (LH-RH) and its functional analogs such as the polypeptides of the formula



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wherein R₁ means His, Tyr, Trp or p-NH₂-Phe; R₂ means Tyr or Phe; R₃ means Gly or a D-amino acid residue; R₄ means Leu, Ile or Nle; R₅ means Gly-NH-R₆ (R₆ is H or a lower alkyl group which may optionally have a hydroxyl group) or NH-R₆ (R₆ is as defined above) and salts thereof [cf. United States Patent No. 3,853,837, No. 4,008,209 and No. 3,972,859, British Patent No. 1,423,083, Proceedings of the National Academy of Sciences of the United States of America 78, 6509-6512, 1981].

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Referring to the above formula (II), the D-amino acid residue R₃ includes, among others, α-D-amino acid residues containing up to 9 carbon atoms (e.g. D-Leu, Ile, Nle, Val, Nval, Abu, Phe, Phg, Ser, Thr, Met, Ala, Trp, α-Aibu, etc.), which may optionally have appropriate substituents (e.g. t-butyl, t-butoxy, t-butoxycarbonyl, etc.). Of course, acid salts and metal complex compounds of peptide (II) can likewise be employed.

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Wherever, in this specification, abbreviations are used to indicate amino acids, peptides, protective groups, etc. in connection with the peptide of formula (II), they are either the abbreviations according to IUPAC-IUB Commission on Biological Nomenclature or those commonly used in this field of art. Furthermore, where any amino acid may exist as optical isomers, the L-isomer is meant unless it is specifically indicated otherwise.

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A representative species is a polypeptide of formula (II) wherein R₁ = His, R₂ = Tyr, R₃ = D-Leu, R₄ = Leu, R₅ = NHCH₂-CH₃.

The polypeptide may also be any of LH-RH antagonist compounds (cf. United States Patent No. 4,086,219, No. 4,124,577, No. 4,253,997 and No. 4,317,815).

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Among further examples of said peptide are insulin, somatostatin, somatostatin derivatives (United States Patent No. 4,087,390, No. 4,093,574, No. 4,100,117, No. 4,253,998), growth hormone, prolactin, adrenocorticotrophic hormone (ACTH), melanocyte stimulating hormone (MSH), thyrotropin-releasing hormone (TRH) and salts and derivatives thereof (Japanese Kokai Patent Application No. 50-121273 and No. 52-116465), thyroid-stimulating hormone (TSH), luteinizing hormone (LH), follicle-stimulating hormone (FSH), vasopressin, vasopressin derivatives [desmopressin, Folia Endocrinologica Japonica, 54, 5, 676-691 (1978)], oxytocin, calcitonin, parathyroid hormone, glucagon, gastrin, secretin, pancreatico-lym, cholecystokinin, angiotensin, human placental lactogen, human chorionic gonadotropin (HCG), enkephalin, enkephalin derivatives [United States Patent No. 4,277,394, European Patent Application Laid-open No. 31567], endorphin, kyotorphin, interferons (α, β and γ), interleukins (I, II, III), taftsin, thymopoietin, thymosin, thymostimulin, thymic humoral factor (THF), thymic serum factor (FTS) as well as derivatives thereof (United States Patent No. 4,229,438) and other thymic factors [Advances in Medicine 125, 10, 835-843 (1983)], tumor necrosis factor (TNF), colony-stimulating factor (CSF), motilin, dynorphin, bombesin, neurotensin, cerulein, bradykinin, urokinase, asparaginase kallikrein, substance P, nerve growth factor, blood-coagulation factor VIII, blood-coagulation factor IX, lysozyme chloride, polymyxin B, colistin, gramicidin, bacitracin, erythropoietin (EPO) and so on.

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Among said antitumor agents may be bleomycin hydrochloride, methotrexate, actinomycin D, mitomycin C, vinblastine sulfate, vincristine sulfate, cisplatin, daunorubicin hydrochloride, adriamycin, neocarzinostatin, cytosine arabinoside, fluorouracil, tetrahydrofuryl-5-fluorouracil, krestin, picibanil, lentinan, levamisole, bestatin, azimexon, glycyrrhizin, poly I:C, poly A:U, poly ICLC and so on.

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Among said antibiotics are gentamicin, dibekacin, kanamycin, lividomycin, tobramycin, amikacin, fradiomycin, sisomicin, tetracycline hydrochloride, oxytetracycline hydrochloride, rolitetracycline, doxycycline hydrochloride, ampicillin, piperacillin, ticarcillin, cephalothin, cephaloridine, cefotiam, cefsulodin, cefmenoxime, cefmetazole, cefazolin, cefotaxime, cefoperazone, ceftizoxime, moxalactam, thienamycin, sulfazecin, azthreonam and so on.

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Among said antipyretics, analgesics and expectorants may be sodium salicylate, sulpyrine, sodium flufenamate, diclofenac sodium, indomethacin sodium, morphine sulfate, pethidine hydrochloride, levorphanol tartrate, oxymorphone and so on. Among said antitussive-expectorants may be included ephedrine hydrochloride, methylephedrine hydrochloride, noscapine hydrochloride, codeine phosphate, dihydrocodeine phosphate, alcloamide hydrochloride, clofedanol hydrochloride, picoperidamine hydrochloride, cloperastine, protokylol hydrochloride, isoproterenol hydrochloride, salbutamol sulfate, terbutaline sulfate, etc. The sedatives may be chlorpromazine hydrochloride, prochlorperazine, trifluoperazine, atropine sulfate, m thylscopolamine bromide and so on. The muscle relaxants may be pridinol methanesulfonate, tubocurarine chloride, pancuronium bromide and so on. The antiepileptics include sodium phenytoin, ethosuximide, acetazolamide sodium, chlordiazepoxide hydrochloride and so on. The antiulcer agents

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include metoclopramide, histidine hydrochloride and so on. The antidepressants include imipramine, clomipramine, nortriptyline, phenelzine sulfate and so on. The antiallergic agents include diphenhydramine hydrochloride, chlorpheniramine maleate, triprolidine hydrochloride, methidiazin hydrochloride, clemizole hydrochloride, diphenylpyraline hydrochloride, methoxyphenamine hydrochloride and so on. The cardiotonics include trans- π -oxocamphor, theophyllin, aminophylline, etilefrine hydrochloride and so on. The antiarrhythmic agents include propranolol hydrochloride, alprenolol hydrochloride, bufetolol vasodilators include oxyfedrine hydrochloride, diltiazem hydrochloride, tolazoline hydrochloride, hexobendine, bamethan sulfate and so on. The hypotensive diuretics include hexamethonium bromide, pentolinium, mecamlamine hydrochloride, ecarazine hydrochloride, clonidine hydrochloride and so on. The antidiabetic agents include glymidine sodium, glipizide, phenformin hydrochloride, buformine hydrochloride, metformin and so on. The anticoagulants include heparin sodium, sodium citrate and so on. The hemostatics include thromboplastin, thrombin, menadione sodium bisulfite, acetomenaphthone, ϵ -aminocaproic acid, tranexamic acid, carbazochrome sodium sulfonate, adrenochrome monoaminoguanidine methansulfonate and so on. The tuberculostats include isoniazid, ethambutol, sodium para-aminosalicylate and so on. The hormones include prednisolone succinate, prednisolone sodium phosphate, dexamethasone sodium sulfate, betamethasone sodium phosphate, hexestrol phosphate, hexestrol acetate, methimazole and so on. The narcotic antagonists include levallorphan tartrate, nalorphine hydrochloride, naloxazone hydrochloride and so on. The bone resorption inhibitors include (sulfur-containing alkyl)aminomethylenebisphosphonic acid and so on. The angiogenesis-inhibiting substances include angiostatic steroid (Science, 221, 719 (1983)), fumagillin (e.g. EP-A-325199, etc.), fumagillol derivatives (e.g. EP-A-357061, EP-A-359036, EP-A-386667, EP-A-415294, etc.) and so on.

The proportion of said water-soluble drug depends on the kind of drug, expected pharmacological effect and its duration etc. but its concentration in the inner aqueous phase of water in oil emulsion in the course of microencapsulation by in water drying process is selected from the range of about 0.001% to about 90% (w/w), preferably 0.01% to 80% (w/w).

The prolonged release preparation of the present invention can be manufactured by the per se known production technology (e.g. see U.S. Patent No 4,652,441). An exemplary manufacturing process comprises preparing a W/O emulsion using an aqueous solution of the water-soluble drug as the inner aqueous phase, to which a drug retaining substance such as gelatin, albumin, pectin or agar is optionally added, and a solution of the prolonged release preparation of the present invention as the oil phase, dispersing said W/O emulsion in an aqueous medium to give a W/O/W emulsion and subjecting the latter to drying in water to give sustained-release microcapsules containing said water-soluble drug.

Such microcapsules can also be manufactured by spray-drying the W/O emulsion.

Other forms of the prolonged release preparation than microcapsules can also be manufactured by melting an appropriate dispersion of the biodegradable composition and molding the melt into beads, rods, needles and other forms.

Dosage forms of administering microcapsules of the present invention include injections, implantations and agents absorbed through mucous membrane of rectum or uterus.

The microcapsules obtained in the above manner are sieved, when necessary after slightly crushing, to eliminate excessively large microcapsules. The average grain size of microcapsules is within the range from about 0.5 to 1000 μ m, desirable and preferably within the range of about 2 to 500 μ m. When the microcapsules are used as injections in the form of suspension, the grain size may be sufficient so long as it satisfies the requirements for dispersability and injectability, for example, desirably within the range of about 2 to 100 μ m.

The microcapsules produced by the methods according to this invention have many advantages. For instance, they scarcely undergo aggregation or cohesion to one another during the production step. There can be obtained microcapsules which are satisfactorily spherical in shape having an optional size. The step of removing the solvent from the oil phase is easy to control, whereby the surface structure of microcapsules, which is decisive for the rate of drug release (inclusive, e.g. of the number and size of pores which are to serve as main routes of drug release), can be controlled.

The microcapsules produced by the method of this invention can be easily administered as injections and implants intramuscularly, subcutaneously, or at an organ, joint cavity or at a lesion such as tumors. They may also be administered in various dosage forms and thus can be used as materials in preparing such dosage forms.

For instance, in making up the microcapsules according to this invention for an injection, the microcapsules according to the invention are dispersed in an aqueous medium together with a dispersing agent (e.g. Tween 80, HCO-60; carboxymethylcellulose, sodium alginate, etc.), a preservative (e.g. methylparaben, propylparaben, etc.), an isotonicizing agent (e.g. sodium chloride, mannitol, sorbitol, glucose, etc.), or suspended in an aqueous medium together with a vegetable oil such as sesame oil or corn oil. Such

dispersion or suspension is formulated into a practically usable sustained-release injection.

Furthermore, the above microencapsulated sustained-release injection can be converted to a more stable, sustained-release injection by adding an additional excipient (e.g. mannitol, sorbitol, lactose, glucose, etc.), redispersing the resulting mixture and effecting solidification by freeze-drying or spray drying with extemporaneous addition of distilled water for injection or some appropriate dispersing agent.

The dose of the sustained-release preparation according to this invention may vary depending on the kind and amount of the water soluble drug, which is the active ingredient, dosage form, duration or drug release, recipient animal (e.g. warm-blooded animals such as mouse, rat, rabbit, sheep, pig, cow, horse, human) and purpose of administration but should be within the range of effective dose of said active ingredient. For example, the single dose per said animal of the microcapsules can adequately be selected within the range of about 0.1 mg to 100 mg/kg body weight, preferably about 0.2 mg to 50 mg/kg body weight.

[Example]

The following comparative and working examples are intended to illustrate the present invention in further detail.

Comparative Example 1

A 1000 ml four-necked flask equipped with nitrogen inlet and condenser lines was charged with 247.7 g of 90% aqueous D,L-lactic acid solution, 95.1 g of glycolic acid and 130.1 g of D,L-2-hydroxybutyric acid and the charge was heated in a nitrogen gas stream at 90 °C and 400 mm Hg to 150 °C and 30 mmHg over 5 hours to remove water as the distillate. The reaction mixture was further heated under reduced pressure at 150-175 °C and 5-7 mmHg for 72 hours, at the end of which time it was cooled to give an amber-colored lactic acid-glycolic acid-2-hydroxybutyric acid copolymer.

This copolymer was dissolved in 1000 ml of dichloromethane and the solution was poured in warm water at 60 °C with stirring. The dough-like polymer precipitate was collected and dried in vacuo at 30 °C.

The peak molecular weight (GPC) of the resulting lactic acid-glycolic acid-2-hydroxybutyric acid copolymer was 12000.

Comparative Example 2

In 0.25 ml of distilled water was dissolved 350 mg of TRH (thyrotropin-releasing hormone) followed by addition of 4.65 g of the lactic acid-glycolic acid-2-hydroxybutyric acid copolymer obtained in Comparative Example 1 as dissolved in 5 ml of dichloromethane. The mixture was stirred with a small homogenizer for 60 seconds to give a W/O emulsion. This emulsion was cooled to 18 °C and poured into 1250 ml of a 0.15% aqueous solution of polyvinyl alcohol (PVA) preadjusted to 19 °C and the mixture was treated with a turbine homogenizer to give a W/O/W emulsion. Then, this W/O/W emulsion was stirred at room temperature to evaporate the dichloromethane and solidify the internal W/O emulsion which was collected by centrifugation. This product was dispersed again in distilled water and centrifuged to wash off the free drug and the like. The collected microcapsules were freeze-dried to give a powder. The result of an in vitro release test of the above microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 1.

Comparative Example 3

In 0.8 ml of distilled water were dissolved 450 mg of leuporelin acetate (TAP-144) and 40 mg of gelatin and the solution was added to a solution of 4.5 g of the lactic acid-glycolic acid-2-hydroxybutyric acid copolymer obtained in Comparative Example 1 in 5 ml of dichloromethane. The mixture was treated with a compact homogenizer for 60 seconds to give a W/O emulsion. This emulsion was cooled to 18 °C and poured in 1200 ml of a 0.15% aqueous solution of polyvinyl alcohol (PVA) preadjusted to 20 °C and the mixture was treated with a turbine homomixer to give a W/O/W emulsion. Then, this W/O/W emulsion was stirred at room temperature to evaporate the dichloromethane and solidify the internal W/O emulsion, followed by centrifugation. This product was redispersed in distilled water and centrifuged again to wash off the free drug and the like.

The microcapsules thus obtained were freeze-dried to give a powder. The result of an in vitro release test of the above microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 2.

Comparative Example 4

A 1,000 ml four-necked flask equipped with nitrogen inlet and condenser means was charged with 247.7 g of 90% aqueous solution of DL-lactic acid and 190.2 g of glycolic acid and the charge was heated in a nitrogen gas stream under reduced pressure at 90 °C/500 mmHg to 150 °C/130 mmHg over 5 hours, with water being constantly distilled off. The reaction mixture was further heated under reduced pressure at 5-7 mmHg/150-180 °C for 28 hours, after which it was cooled to give an amber-colored lactic acid-glycolic acid copolymer.

The copolymer thus obtained was dissolved in 1,000 ml of dichloromethane and the solution was poured in warm water at 60 °C with stirring. The resulting dough-like high polymer precipitate was collected and dried in vacuo at 30 °C.

The peak molecular weight of the resulting lactic acid-glycolic acid copolymer as determined by GPC was 12,000.

Comparative Example 5

In 0.8 ml of distilled water were dissolved 450 mg of leuporelin acetate (TAP-144) and 40 mg of gelatin and the solution was added to a solution prepared by dissolving 4.5 g of a 1:1 mixture of the lactic acid-glycolic copolymer of Comparative Example 4 and the polylactic acid of Reference Example 1 in 5 ml of dichloromethane. The mixture was homogenized with a compact homogenizer for 60 second to give a W/O emulsion. This emulsion had the tendency to separate into two layers. This emulsion was cooled to 18 °C and poured in 1,200 ml of 0.15% aqueous solution of polyvinyl alcohol (PVA) preadjusted to 20 °C. The mixture was homogenized with a turbine homomixer to give a W/O/W emulsion. Then, while this W/O/W emulsion was stirred at room temperature, the dichloromethane was evaporated to solidify the internal W/O emulsion which was then collected by centrifugation. This emulsion was redispersed in distilled water and further centrifuged to wash out the free drug, etc.

The collected microcapsules were lyophilized to give a powder. The result of the *in vitro* release test of the microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 2.

Reference Example 1

A 1000 ml four-necked flask equipped with nitrogen inlet and condenser lines was charged with 495.4 g of a 90% aqueous solution of D,L-lactic acid and the charge was heated under reduced pressure in a nitrogen gas stream at 90 °C and 400 mmHg ~ 150 °C and 30 mmHg over 5 hours to remove water as the distillate. The reaction mixture was further heated under reduced pressure at 5-7 mmHg and 150 ~ 175 °C for 65 hours and, then, cooled to give an amber-colored polylactic acid.

This polymer was dissolved in 1000 ml of dichloromethane and added to warm water at 60 °C with stirring. The doughy polymer precipitate was collected and dried in vacuo at 30 °C.

The peak molecular weight of the resulting polylactic acid as determined by GPC was 16000.

Reference Example 2

A 1000 ml four-necked flask equipped with nitrogen inlet and condenser lines was charged with 190.2 g of glycolic acid and 260.2 g of D,L-2-hydroxybutyric acid and the charge was heated under reduced pressure in a nitrogen gas stream at 90 °C and 400 mmHg ~ 150 °C and 30 mmHg over 5 hours to remove water as the distillate. The reaction mixture was further heated under reduced pressure at 5-7 mmHg and 150-175 °C for 72 hours and, then, cooled to give an amber-colored glycolic acid-2-hydroxybutyric acid copolymer.

This copolymer was dissolved in 1000 ml of dichloromethane and added to warm water at 60 °C with stirring. The doughy polymer precipitate was collected and dried in vacuo at 30 °C.

The peak molecular weight of this glycolic acid-2-hydroxybutyric acid copolymer as determined by GPC was 10000.

Reference Example 3

A 1,000 ml four-necked flask equipped with nitrogen inlet and condenser means was charged with 300 g of 90% aqueous solution of D,L-lactic acid and 100 g of 90% L-lactic acid and the charge was heated in a nitrogen gas stream under reduced pressure at 100 °C/500 mmHg to 150 °C/30 mmHg over 4 hours, with

water being constantly distilled off. The reaction mixture was heated under reduced pressure at 5-7 mmHg/150-180 °C for 24 hours, after which it was cooled to give an amber-colored lactic acid polymer.

This polymer was dissolved in 1,000 ml of dichloromethane and the solution was poured in warm water at 60 °C with stirring. The dough-like polymer precipitate was collected and dried in vacuo at 30 °C.

As determined by GPC, the peak molecular weight value of this lactic acid polymer was 7,000.

Reference Example 4

A 1,000 ml four-necked flask equipped with nitrogen inlet and condenser means was charged with 145.8 g of D,L-2-hydroxybutyric acid and 177.7 g of glycolic acid and the charge was heated in a nitrogen gas stream under reduced pressure at 100 °C/500 mmHg to 150 °C/30 mmHg over 3.5 hours, with water being constantly distilled off. The reaction mixture was further heated under reduced pressure at 5-7 mmHg/150-180 °C for 27 hours, followed by cooling to give an amber-colored glycolic acid-2-hydroxybutyric acid copolymer.

This copolymer was dissolved in 1,000 ml of dichloromethane and the solution was poured in warm water at 60 °C with stirring. The resulting dough-like polymer precipitate was collected and dried in vacuo at 25 °C.

As determined by GPC, the peak molecular weight value of this glycolic acid-2-hydroxybutyric acid copolymer was 14,000.

Example 1

Using a 3:1 (w/w) mixture of the polylactic acid prepared in Reference Example 1 and the glycolic acid-2-hydroxybutyric acid copolymer prepared in Reference Example 1, the procedure of Comparative Example 2 was followed to prepare microcapsules. The result of an *in vitro* release test of the above microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 1.

Example 2

Using a 1:1 (w/w) mixture of the polylactic acid prepared in Reference Example 1 and the glycolic acid-2-hydroxybutyric acid copolymer prepared in Reference Example 2, the procedure of Comparative Example 2 was followed to prepare microcapsules. The result of an *in vitro* release test of the above microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 1.

Example 3

Using a 1:3 (w/w) mixture of the polylactic acid prepared in Reference Example 1 and the glycolic acid-2-hydroxybutyric acid copolymer obtained in Reference Example 2, the procedure of Comparative Example 2 was followed to prepare microcapsules. The result of an *in vitro* release test of the above microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 1.

Table 1

	Percent residue of TRH, (%) ^{a)}						
	One day	One week	Two weeks	Three weeks	Four weeks	Five weeks	Six weeks
Comparative Example 2	95.1	79.8	50.1	2.9			
Example 1	97.0	86.8	70.2	52.1	34.8	16.2	0.7
Example 2	95.7	76.8	52.0	24.3	3.1		
Example 3	93.3	62.0	21.7	0.1			

a) 1/30 M phosphate buffer, pH 7.0, 37 °C

It is apparent from Table 1 that the release period can be adjusted to 6, 4 and 3 weeks, respectively, by varying the blending ratio between polylactic acid (A) and glycolic acid-2-hydroxybutyric acid copolymer (B). Furthermore, whereas the microcapsules of Comparative Example 2 cannot release the drug at constant rate, all the microcapsules of the invention can release the drug at substantially constant rate.

Example 4

Using a 3:1 (w/w) mixture of the polylactic acid prepared in Reference Example 1 and the glycolic acid-2-hydroxybutyric acid copolymer prepared in Reference Example 2, the procedure of Comparative Example 3 was followed to prepare microcapsules. The result of an *in vitro* release test of these microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 2.

Example 5

Using a 1:1 mixture of the polylactic acid prepared in Reference Example 1 and the glycolic acid-2-hydroxybutyric acid copolymer prepared in Reference Example 2, the procedure of Comparative Example 3 was followed to prepare microcapsules. The result of an *in vitro* release test of the above microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 2.

Example 6

Using a 1:3 (w/w) mixture of the polylactic acid prepared in Reference Example 1 and the glycolic acid-2-hydroxybutyric acid copolymer prepared in Reference Example 2, the procedure of Comparative Example 3 was followed to prepare microcapsules. The result of an *in vitro* release test of these microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 2.

Table 2

	Percent residue of TAP-144 (%) ^{a)}						
	One day	One week	Two weeks	Three weeks	Four weeks	Five weeks	Six weeks
Comparative Example 3	93.8	76.2	57.1	19.5	0.1		
Comparative Example 5	50.7	41.7	23.8	11.7	5.4	3.4	
Example 4	97.2	88.1	72.3	56.1	38.4	23.7	6.0
Example 5	96.1	77.8	56.0	36.8	15.0	0.1	
Example 6	94.1	60.6	24.3	0.1			

a) 1/30 M phosphate buffer, pH 7.0, 37 °C

It is apparent from Table 2 that the release period can be adjusted to the desirous period by varying the blending ratio of polylactic acid (A) to glycolic acid-2-hydroxybutyric acid copolymer (B). Whereas the drug release rate from the microcapsules of Comparative Example 3 was not constant, all the microcapsules of the present invention can release the drug at a substantially constant rate over the entire period. As shown for Comparative Example 5, the combination of polylactic acid (A) and lactic acid-glycolic acid copolymer (B) did not achieve the effect of the invention.

Example 7

In 0.4 ml of distilled water was dissolved 400 mg of leuporelin acetate (TAP-144) and the solution was added to a solution prepared by dissolving 4.0 g of a 1:1 mixture of the polylactic acid of Reference Example 3 and the glycolic acid-2-hydroxybutyric acid copolymer of Reference Example 4 in 5 ml of dichloromethane. The mixture was homogenized with a compact homogenizer for 60 seconds to give a W/O emulsion. This emulsion was cooled to 18 °C and poured in 1,000 ml of a 0.1% aqueous solution of polyvinyl alcohol (PVA) preadjusted to 20 °C. The mixture was homogenized with a turbine homomixer to give a W/O/W emulsion. Then, while this W/O/W emulsion was stirred at room temperature, the dichloromethane was evaporated to solidify the internal W/O emulsion which was then collected by centrifugation. This emulsion was redispersed in distilled water and further centrifuged to wash out the free drug, etc.

The collected microcapsules were lyophilized to give a powder. The result of the *in vitro* release test of the microcapsules in phosphate buffer (pH 7.0) at 37 °C is shown in Table 3.

Table 3

	Percent residue of TAP-144 (%) ^{a)}					
	One day	One week	Two weeks	Three weeks	Four weeks	Five weeks
Example 7	91.9	60.1	29.1	9.3	1.8	0.2

a) 1/30 M phosphate buffer, pH 7.0, 37 ° C

When a prolonged release therapeutic system is manufactured using the prolonged release pharmaceutical base comprising a blend of a polylactic acid and a glycolic acid copolymer in accordance with the present invention, the drug release period of the therapeutic system can be freely controlled by varying the blending ratio. Furthermore, the drug is released at a constant rate over the total release period without a large burst at the initial stage.

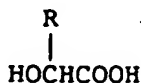
Claims

1. A polymer composition for a prolonged release preparation which comprises
(A) a polylactic acid and
(B) a copolymer of glycolic acid and a hydroxycarboxylic acid of the formula



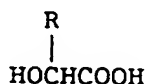
wherein R stands for an alkyl group having 2 to 8 carbons, and wherein the weight ratio of (A) and (B) is in the range of 10/90 through 90/10.

2. The polymer composition according to claim 1, wherein the polylactic acid is a polymer of D-lactic acid and L-lactic acid.
3. The polymer composition according to claim 1, wherein the polylactic acid is a polymer of D-lactic acid and L-lactic acid, and the mole ratio of D- and L-lactic acid is 45/55 to 25/75.
4. The polymer composition according to claim 1, wherein the polylactic acid has a molecular weight peak value of 5000 to 30000 as determined by GPC.
5. The polymer composition according to claim 1, wherein the hydroxycarboxylic acid is a member selected from the group consisting of 2-hydroxybutyric acid, 2-hydroxyvaleric acid, 2-hydroxy-3-methylbutyric acid, 2-hydroxycaproic acid, 2-hydroxyisocaproic acid and 2-hydroxycaprylic acid.
6. The polymer composition according to claim 1, wherein the copolymer is a copolymer in which the proportion of glycolic acid is in the range of 40 to 70 mole% and the proportion of the said hydroxycarboxylic acid is 60 to 30 mole%, respectively.
7. The polymer composition according to claim 1, wherein the copolymer has a molecular weight peak value of 5000 to 20000 as determined by GPC.
8. A method of producing a polymer composition for a prolonged release preparation which comprises mixing
(A) a polylactic acid and
(B) a copolymer of glycolic acid and a hydroxycarboxylic acid of the formula



wherein R stands for an alkyl group having 2 to 8 carbons, in a weight ratio of 10/90 to 90/10.

9. The method according to claim 8, wherein the polylactic acid is a polymer of D-lactic acid and L-lactic acid.
10. The method according to claim 8, wherein the polylactic acid is a polymer of D-lactic acid and L-lactic acid, and the mole ratio of D- and L-lactic acid is 45/55 to 25/75.
11. The method according to claim 8, wherein the polylactic acid has a molecular weight peak value of 5000 to 30000 as determined by GPC.
12. The method according to claim 8, wherein the hydroxycarboxylic acid is a member selected from the group consisting of 2-hydroxybutyric acid, 2-hydroxyvaleric acid, 2-hydroxy-3-methylbutyric acid, 2-hydroxycaproic acid, 2-hydroxyisocaproic acid and 2-hydroxycaprylic acid.
13. The method according to claim 8, wherein the copolymer is a copolymer in which the proportion of glycolic acid is in the range of 40 to 70 mole% and the proportion of the said hydroxycarboxylic acid is in the range of 60 to 30 mole%, respectively.
14. The method according to claim 8, wherein the copolymer has a molecular weight peak value of 5000 to 20000 as determined by GPC.
15. A prolonged release preparation which comprises a water-soluble drug being dispersed in a polymer composition for a prolonged release preparation comprising
 - (A) a polylactic acid and
 - (B) a copolymer of glycolic acid and a hydroxycarboxylic acid of the formula



wherein R stands for an alkyl group having 2 to 8 carbons, and wherein the weight ratio of (A) and (B) is in the range of 10/90 through 90/10.

16. The prolonged release preparation according to claim 15, wherein the polylactic acid is a polymer of D-lactic acid and L-lactic acid.
17. The prolonged release preparation according to claim 15, wherein the polylactic acid is a polymer of D-lactic acid and L-lactic acid, the mole ratio of D- and L-lactic acid is 45/55 to 25/75.
18. The prolonged release preparation according to claim 15, wherein the polylactic acid has a molecular weight peak value of 5000 to 30000 as determined by GPC.
19. The prolonged release preparation according to claim 15, wherein the hydroxycarboxylic acid is a member selected from the group consisting of 2-hydroxybutyric acid, 2-hydroxyvaleric acid, 2-hydroxy-3-methylbutyric acid, 2-hydroxycaproic acid, 2-hydroxyisocaproic acid and 2-hydroxycaprylic acid.
20. The prolonged release preparation according to claim 15, wherein the copolymer is a copolymer in which the proportion of glycolic acid is in the range of 40 to 70 mole% the proportion of the said hydroxycarboxylic acid is in the range of 60 to 30 mole%, respectively.
21. The prolonged release preparation according to claim 15, wherein the copolymer has a molecular weight peak value of 5000 to 20000 as determined by GPC.
22. The prolonged release preparation according to claim 15, wherein the water-soluble drug is a physiologically active polypeptide.

23. The prolonged release preparation according to claim 22, wherein the physiologically active polypeptide is leuteinizing hormone-releasing hormone or its functional analogs.

24. The prolonged release preparation according to claim 23, wherein the functional analogs of leuteinizing hormone-releasing hormone are compounds of the formula



wherein R_1 means His, Tyr, Trp or $p-NH_2$ -Phe; R_2 means Tyr or Phe; R_3 means Gly or a D-amino acid residue; R_4 means Leu, Ile or Nle; R_5 means $Gly-NH-R_6$ (R_6 is H or a lower alkyl group which may optionally have hydroxyl group) or $NH-R_6$ (R_6 is as defined above) or salts thereof.

25. The prolonged release preparation according to claim 22, wherein the physiologically active polypeptide is (Pyr)Glu-His-Trp-Ser-Tyr-D-Leu-Leu-Arg-Pro- $NH-C_2H_5$ or acetate thereof.

Patentansprüche

1. Polymerzusammensetzung für ein Präparat mit verlängerter Freisetzung, die umfaßt:

(A) eine Polymilchsäure und

(B) ein Copolymer aus Glykolsäure und einer Hydroxycarbonsäure der Formel



worin R für eine Alkylgruppe mit 2 - 8 Kohlenstoffatomen steht und das Gewichtsverhältnis von (A) zu (B) im Bereich von 10/90 bis 90/10 inklusive liegt.

2. Polymerzusammensetzung nach Anspruch 1, worin die Polymilchsäure ein Polymer aus D-Milchsäure und L-Milchsäure ist.

3. Polymerzusammensetzung nach Anspruch 1, worin die Polymilchsäure ein Polymer aus D-Milchsäure und L-Milchsäure ist und das Molverhältnis von D- zu L-Milchsäure 45/55 bis 25/75 beträgt.

4. Polymerzusammensetzung nach Anspruch 1, worin die Polymilchsäure einen durch GPC bestimmten Molekulargewichts-Spitzenwert von 5.000 bis 30.000 aufweist.

5. Polymerzusammensetzung nach Anspruch 1, worin die Hydroxycarbonsäure ein Vertreter der Gruppe, bestehend aus 2-Hydroxybuttersäure, 2-Hydroxyvaleriansäure, 2-Hydroxy-3-methylbuttersäure, 2-Hydroxycapronsäure, 2-Hydroxyisocapronsäure und 2-Hydroxycaprylsäure, ist.

6. Polymerzusammensetzung nach Anspruch 1, worin das Copolymer ein Copolymer ist, worin jeweils der Anteil von Glykolsäure im Bereich von 40 bis 70 Mol-% liegt und der Anteil der Hydroxycarbonsäure 60 bis 30 Mol-% beträgt.

7. Polymerzusammensetzung nach Anspruch 1, worin das Copolymer einen durch GPC bestimmten Molekulargewichts-Spitzenwert von 5.000 bis 20.000 aufweist.

8. Verfahren zur Herstellung einer Polymerzusammensetzung für ein Präparat mit verlängerter Freisetzung, das umfaßt: das Vermischen
(A) einer Polymilchsäure und

(B) eines Copolymers aus Glykolsäure und einer Hydroxycarbonsäure der Formel



worin R für eine Alkylgruppe mit 2 - 8 Kohlenstoffatomen steht, in einem Gewichtsverhältnis im Bereich von 10/90 bis 90/10.

- 10
9. Verfahren nach Anspruch 8, worin die Polymilchsäure ein Polymer aus D-Milchsäure und L-Milchsäure ist.
- 15
10. Verfahren nach Anspruch 8, worin die Polymilchsäure ein Polymer aus D-Milchsäure und L-Milchsäure ist und das Molverhältnis von D- zu L-Milchsäure 45/55 bis 25/75 beträgt.
11. Verfahren nach Anspruch 8, worin die Polymilchsäure einen durch GPC bestimmten Molekulargewichts-Spitzenwert von 5.000 bis 30.000 aufweist.
- 20
12. Verfahren nach Anspruch 8, worin die Hydroxycarbonsäure ein Vertreter der Gruppe, bestehend aus 2-Hydroxybuttersäure, 2-Hydroxyvaleriansäure, 2-Hydroxy-3-methylbuttersäure, 2-Hydroxycapronsäure, 2-Hydroxyisocapronsäure und 2-Hydroxycaprylsäure, ist.
- 25
13. Verfahren nach Anspruch 8, worin das Copolymer ein Copolymer ist, worin jeweils der Anteil von Glykolsäure im Bereich von 40 bis 70 Mol-% und der Anteil der Hydroxycarbonsäure im Bereich von 60 bis 30 Mol-% liegt.
14. Verfahren nach Anspruch 8, worin das Copolymer einen durch GPC bestimmten Molekulargewichts-Spitzenwert von 5.000 bis 20.000 aufweist.
- 30
15. Präparat mit verlängerter Freisetzung, das umfaßt: einen wasserlöslichen Arzneimittelwirkstoff, der in einer Polymerzusammensetzung für ein Präparat mit verlängerter Freisetzung dispergiert ist, die umfaßt:
- 35
- (A) eine Polymilchsäure und
- (B) ein Copolymer aus Glykolsäure und einer Hydroxycarbonsäure der Formel



worin R für eine Alkylgruppe mit 2 - 8 Kohlenstoffatomen steht und das Gewichtsverhältnis von (A) zu (B) im Bereich von 10/90 bis 90/10 inklusive liegt.

- 45
16. Präparat mit verlängerter Freisetzung nach Anspruch 15, worin die Polymilchsäure ein Polymer aus D-Milchsäure und L-Milchsäure ist.
- 50
17. Präparat mit verlängerter Freisetzung nach Anspruch 15, worin die Polymilchsäure ein Polymer aus D-Milchsäure und L-Milchsäure ist und das Molverhältnis von D- zu L-Milchsäure 45/55 bis 25/75 beträgt.
18. Präparat mit verlängerter Freisetzung nach Anspruch 15, worin die Polymilchsäure einen durch GPC bestimmten Molekulargewichts-Spitzenwert von 5.000 bis 30.000 aufweist.
- 55
19. Präparat mit verlängerter Freisetzung nach Anspruch 15, worin die Hydroxycarbonsäure ein Vertreter der Gruppe, bestehend aus 2-Hydroxybuttersäure, 2-Hydroxyvaleriansäure, 2-Hydroxy-3-methylbuttersäure, 2-Hydroxycapronsäure, 2-Hydroxyisocapronsäure und 2-Hydroxycaprylsäure, ist.

20. Préparat mit verlängerter Freisetzung nach Anspruch 15, worin das Copolymer ein Copolymer ist, worin jeweils der Anteil von Glykolsäure im Bereich von 40 bis 70 Mol-% und der Anteil der Hydroxycarbonsäure im Bereich von 60 bis 30 Mol-% liegt.
- 5 21. Préparat mit verlängerter Freisetzung nach Anspruch 15, worin das Copolymer einen durch GPC bestimmten Molekulargewichts-Spitzenwert von 5.000 bis 20.000 aufweist.
22. Préparat mit verlängerter Freisetzung nach Anspruch 15, worin der wasserlösliche Arzneimittelwirkstoff ein physiologisch wirksames Polypeptid ist.
- 10 23. Préparat mit verlängerter Freisetzung nach Anspruch 22, worin das physiologisch wirksame Polypeptid ein leuteinisierendes Hormon freisetzendes Hormon oder dessen funktionale Analogen ist.
- 15 24. Préparat mit verlängerter Freisetzung nach Anspruch 23, worin die funktionalen Analogen des ein leuteinisierendes Hormon freisetzenden Hormons Verbindungen der Formel
- (Pyr)Glu-R₁-Trp-Ser-R₂-R₃-R₄-Arg-Pro-R₅
- 20 sind, worin R₁ His, Tyr, Trp oder p-NH₂-Phe bedeutet; R₂ Tyr oder Phe bedeutet; R₃ Gly oder einen D-Aminosäurerest bedeutet; R₄ Leu, Ile oder Nle bedeutet; und R₅ Gly-NH-R₆ bedeutet (wobei R₆ = H oder eine niedere Alkylgruppe, die gegebenenfalls eine Hydroxylgruppe besitzen kann, ist) oder NH-R₆ (wobei R₆ wie zuvor definiert ist) bedeutet oder Salze davon sind.
- 25 25. Préparat mit verlängerter Freisetzung nach Anspruch 22, worin das physiologisch wirksame Polypeptid (Pyr)Glu-His-Trp-Ser-Tyr-D-Leu-Leu-Arg-Pro-NH-C₂H₅ oder ein Acetat davon ist.

Revendications

1. Composition de polymères pour une préparation à libération prolongée, qui comprend
- 30 (A) un acide polylactique et
(B) un copolymère d'acide glycolique et d'un acide hydroxycarboxylique de formule



dans laquelle R représente un groupe alcoyle comportant de 2 à 8 atomes de carbone, et dans laquelle le rapport pondéral de (A) et de (B) se situe dans la plage de 10/90 à 90/10.

- 40 2. Composition de polymères selon la revendication 1, dans laquelle l'acide polylactique est un polymère de l'acide D-lactique et de l'acide L-lactique.
- 45 3. Composition de polymères selon la revendication 1, dans laquelle l'acide polylactique est un polymère de l'acide D-lactique et de l'acide L-lactique, et le rapport molaire de l'acide D-lactique et de l'acide L-lactique est de 45/55 à 25/75.
- 50 4. Composition de polymères selon la revendication 1, dans laquelle l'acide polylactique a une valeur de pointe du poids moléculaire de 5000 à 30000 selon détermination par chromatographie en phase gazeuse (CPG).
- 55 5. Composition de polymères selon la revendication 1, dans laquelle l'acide hydroxycarboxylique est choisi dans le groupe consistant en l'acide 2-hydroxybutyrique, l'acide 2-hydroxyvalérique, l'acide 2-hydroxy-3-méthylbutyrique, l'acide 2-hydroxycaproïque, l'acide 2-hydroxyisocaproïque et l'acide 2-hydroxycaprylique.
6. Composition de polymères selon la revendication 1, dans laquelle le copolymère est un copolymère dans lequel la proportion d'acide glycolique se situe dans la plage de 40 à 70 mol % et la proportion

dudit acide hydroxycarboxylique est de 60 à 30 mole%, respectivement.

7. Composition de polymères selon la revendication 1, dans laquelle le copolymère a une valeur de pointe du poids moléculaire de 5000 à 20000 selon détermination par CPG.

8. Procédé de préparation d'une composition de polymères pour une préparation à libération prolongée, selon lequel on mélange
(A) un acide polylactique et
(B) un copolymère d'acide glycolique et d'un acide hydroxycarboxylique de formule



dans laquelle R représente un groupe alcoyle comportant de 2 à 8 atomes de carbone, en un rapport pondéral de 10/90 à 90/10.

9. Procédé selon la revendication 8, dans lequel l'acide polylactique est un polymère de l'acide D-lactique et de l'acide L-lactique.

10. Procédé selon la revendication 8, dans lequel l'acide polylactique est un polymère de l'acide D-lactique et de l'acide L-lactique, et le rapport molaire de l'acide D-lactique et de l'acide L-lactique est de 45/55 à 25/75.

11. Procédé selon la revendication 8, dans lequel l'acide polylactique a une valeur de pointe du poids moléculaire de 5000 à 30000 selon détermination par chromatographie en phase gazeuse (CPG).

12. Procédé selon la revendication 8, dans lequel l'acide hydroxycarboxylique est choisi dans le groupe consistant en l'acide 2-hydroxybutyrique, l'acide 2-hydroxyvalérique, l'acide 2-hydroxy-3-méthylbutyrique, l'acide 2-hydroxycaproïque, l'acide 2-hydroxyisocaproïque et l'acide 2-hydroxycaprylique.

13. Procédé selon la revendication 8, dans lequel le copolymère est un copolymère dans lequel la proportion d'acide glycolique se situe dans la plage de 40 à 70 mole% et la proportion dudit acide hydroxycarboxylique se situe dans la plage de 60 à 30 mole%, respectivement.

14. Procédé selon la revendication 8, dans lequel le copolymère a une valeur de pointe du poids moléculaire de 5000 à 20000 selon détermination par CPG.

15. Préparation à libération prolongée, qui comprend un médicament soluble dans l'eau en dispersion dans une composition de polymères pour une préparation à libération prolongée qui comprend
(A) un acide polylactique et
(B) un copolymère d'acide glycolique et d'un acide hydroxycarboxylique de formule



dans laquelle R représente un groupe alcoyle comportant de 2 à 8 atomes de carbone, et dans laquelle le rapport pondéral de (A) et de (B) se situe dans la plage de 10/90 à 90/10.

16. Préparation à libération prolongée selon la revendication 15, dans laquelle l'acide polylactique est un polymère de l'acide D-lactique et de l'acide L-lactique.

17. Préparation à libération prolongée selon la revendication 15, dans laquelle l'acide polylactique est un polymère de l'acide D-lactique et de l'acide L-lactique, et le rapport molaire de l'acide D-lactique et de

l'acide L-lactique est de 45/55 à 25/75.

18. Préparation à libération prolongée selon la revendication 15, dans laquelle l'acide polylactique a une
 5 valeur de pointe du poids moléculaire de 5000 à 30000 selon détermination par chromatographie en
 phase gazeuse (CPG).
19. Préparation à libération prolongée selon la revendication 15, dans laquelle l'acide hydroxycarboxylique
 est choisi dans le groupe consistant en l'acide 2-hydroxybutyrique, l'acide 2-hydroxyvalérique, l'acide
 10 2-hydroxy-3-méthylbutyrique, l'acide 2-hydroxycaproïque, l'acide 2-hydroxyisocaproïque et l'acide 2-
 hydroxycaprylique.
20. Préparation à libération prolongée selon la revendication 15, dans laquelle le copolymère est un
 copolymère dans lequel la proportion d'acide glycolique se situe dans la plage de 40 à 70 mole% et la
 15 proportion dudit acide hydroxycarboxylique se situe dans la plage de 60 à 30 mole%, respectivement.
21. Préparation à libération prolongée selon la revendication 15, dans laquelle le copolymère a une valeur
 de pointe du poids moléculaire de 5000 à 20000 selon détermination par CPG.
22. Préparation à libération prolongée selon la revendication 15, dans laquelle le médicament soluble dans
 20 l'eau est un polypeptide physiologiquement actif.
23. Préparation à libération prolongée selon la revendication 22, dans laquelle le polypeptide physiologi-
 quement actif est l'hormone libérant l'hormone lutéinisante ou un analogue fonctionnel de celle-ci.
24. Préparation à libération prolongée selon la revendication 23, dans laquelle l'analogue fonctionnel de
 25 l'hormone libérant l'hormone lutéinisante est un composé de formule



- 30 dans laquelle R₁ représente His, Tyr, Trp ou p-NH₂-Phe; R₂ représente Tyr ou Phe; R₃ représente Gly
 ou un radical d'acide aminé D; R₄ représente Leu, Ile ou Nle; R₅ représente Gly-NH-R₆ (R₆ représentant
 l'hydrogène ou un groupe alcoyle inférieur qui peut comporter éventuellement un groupe hydroxyle) ou
 NH-R₆ (R₆ étant tel que défini ci-dessus), ou un sel de celui-ci.
- 35 25. Préparation à libération prolongée selon la revendication 22, dans laquelle le polypeptide physiologi-
 quement actif est (Pyr)Glu-His-Trp-Ser-Tyr-D-Leu-Leu-Arg-Pro-NH-C₂H₅ ou un acétate de celui-ci.